

**AMENDMENT TO THE SPECIFICATION**

**Please add the following paragraphs starting on page 21 at line 28 with the following new paragraphs.**

--FIG. 27 is a perspective view of an implantable medical device to which a feedthrough according to the present invention is electrically coupled.

FIG. 28a is a partial perspective view of an implantable medical device to which a feedthrough according to the present invention is electrically coupled.

FIG. 28b is a perspective view of an embodiment of a feedthrough according to the present invention.

FIG. 28c is a partial perspective view of an implantable medical device after a feedthrough according to the present invention has been electrically coupled.--

**Please replace the paragraph beginning at page 22, line 11 with the following paragraph.**

Following removal of the sacrificial component of the conductive structure, the green body of the insulator can undergo a step of debinding 14 prior to a step of sintering 15. Once sintered, the ceramic feedthrough with the conductive members extending therethrough is ready for appropriate mounting in the wall 278 of an implantable stimulator unit 276 of a cochlear implant hearing prosthesis 270 or other appropriate device.

**Please replace the paragraph beginning at page 30, line 24 with the following paragraph.**

Such a feedthrough as depicted in FIG. 21 can be adapted to be brazed into the wall 278 of an implantable stimulator unit of a cochlear implant hearing prosthesis 270. In this regard, the feedthrough can be adapted to provide electrical conduction between the circuitry within the implantable stimulator unit 276 and the intracochlear or extracochlear electrodes 272, and/or the implantable receiver coil 280.

**Please replace the paragraph beginning at page 30, line 30 with the following paragraph.**

An advantage of the present invention is that it provides the possibility of allowing exchange of an implantable stimulator unit 276 within a recipient with a newer or replacement model without the necessity to explant the intracochlear electrode array 274. For example, if a recipient already has an implanted stimulator unit 276 with a cochlear array 274 connected thereto and electrical connection provided by a feedthrough, it is possible to disconnect the electrode array 274 from the external side of the feedthrough and then remove the stimulator unit 276. While a newer model stimulator unit 276 may have a different internal and/or external construction, a feedthrough as here depicted can be provided in the housing of the stimulator unit that is connectable on its external side with the existing configuration of the implanted cochlear array 274 but has a different configuration on its internal side that is compatible with the configuration of the internal wiring of the stimulator unit 276.

**Please replace the paragraph beginning at page 32, line 10 with the following paragraph.**

Such a feedthrough can be adapted to be brazed into the wall 278 of an implantable stimulator unit 276 of a cochlear implant hearing prosthesis 270. In this embodiment, the feedthrough can be adapted to provide electrical conduction between the circuitry within the

implantable stimulator unit 276 and the intracochlear or extracochlear electrodes 272, and/or the implantable receiver coil 280.

**Please replace the paragraph beginning at page 32, line 16 with the following paragraph.**

Each feedthrough preferably has sufficient platinum members embedded therein to ensure there are sufficient connectors for each of the electrode channels of the intracochlear electrode array 274, one or more extracochlear electrodes, and the inputs from the receiver coil 280.